

## Streak Artifact Reduction in Human-scale Dark-field CT Using 3D Gaussian Splatting

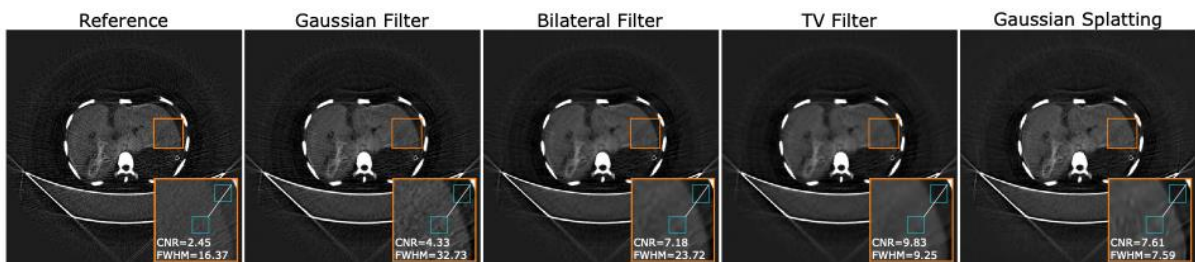
**Objective** – Functional imaging of the lung is enabled by measuring small-angle scattering at tissue interfaces using X-ray dark-field computed tomography (DFCT). However, image quality is typically limited by hardware constraints inherent to the setup. We propose a post-processing method based on the 3D Gaussian Splatting (3DGS) [2] method to improve DFCT image quality.

**Motivation & Background** – The clinical DFCT scanner enables attenuation- and small-angle scatter-based imaging of human-scale phantoms. Due to the scanner’s vibrating Talbot-Lau grating interferometer, images suffer from inherent streak artifacts [1]. In this work, DFCT data is processed by re-purposing the 3DGS method, designed for rendering sparsely sampled X-ray attenuation data [2], and is compared against conventional filtering.

**Methods** – A ventilated ex vivo porcine lung sample placed inside an anthropomorphic Lungman phantom (Kyoto Kagaku, Tokyo, Japan), measured at 20 randomly selected table positions, and reconstructed with the filtered back-projection algorithm at the clinical DFCT setup [1] was utilized. Gaussian, bilateral, and total variation (TV) filters, and the re-purposed 3DGS model from [2] were explored for post-processing DFCT data. For each conventional filter, the hyperparameters were optimized via grid search, maximizing the structural similarity index between 3DGS and the filtered image on a global image-level. The contrast-to-noise ratio (CNR) and the full-width-at-half-maximum (FWHM) of manually-selected  $20 \times 20$  pixel regions of lung tissue and air were calculated, as in Fig. 1.

**Results** – The resulting mean and standard deviation values are: for the reference scan (CNR =  $2.44 \pm 0.93$ , FWHM =  $40.25 \pm 11.32$ ), Gaussian filter (CNR =  $4.14 \pm 1.48$ , FWHM =  $31.99 \pm 16.22$ ), bilateral filter (CNR =  $6.44 \pm 2.60$ , FWHM =  $23.36 \pm 16.33$ ), TV (CNR =  $8.09 \pm 3.47$ , FWHM =  $15.78 \pm 16.21$ ), and 3DGS (CNR =  $6.74 \pm 2.51$ , FWHM =  $10.06 \pm 8.83$ ).

**Conclusion** – These findings indicate that 3DGS outperforms conventional filtering in DFCT streak-reduction, preserving edge sharpness and a high CNR, a necessity for diagnostic accuracy in future clinical trials.



**Fig. 1.** Example axial DFCT slice, without (reference) and with streak-reduction post-processing. The CNR and FWHM values for the  $20 \times 20$  pixel lung tissue and air regions (blue) are provided. The white line is used for pixel-wise FWHM calculation.

## References

- [1] M. Viermetz et al., “Dark-field computed tomography reaches the human scale,” *PNAS*, vol. 119, 2022.
- [2] R. Zha et al., “R<sup>2</sup>-gaussian: Rectifying radiative gaussian splatting for tomographic reconstruction,” *Advances in Neural Information Processing Systems*, vol. 37, 2024.